

Immediate effects of wearing knee length socks differing in compression level on postural regulation in community-dwelling, healthy, elderly men and women

WOO, Mei Teng, DAVIDS, Keith <<http://orcid.org/0000-0003-1398-6123>>, LIUKKONEN, Jarmo, CHOW, Jia Yi and JAAKKOLA, Timo

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2 **postural regulation in community-dwelling, healthy, elderly men and women**

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1 Postural regulation and stability of balance are affected by types of standing surfaces
2 and somatosensory system function of an individual (Patel et al., 2008). Standing on unstable
3 surfaces, like foam surfaces, have revealed the important role of somatosensory information
4 in postural regulation and balance (Patel et al. 2008; Qiu et al., 2012). Studies have suggested
5 that postural sway increases for balance regulation, especially when individuals are standing
6 on a foam surface (Patel et al., 2008; Vuillerman & Pinsault, 2007). Somatosensory function
7 is important to study since neurodegeneration can result in age-related declines in postural
8 regulation due to reduction in cognitive and sensory system capacities (Rose, 2012). For
9 example, ageing can result in decreased sensitivity to sensory information and motor output,
10 slowing of cognitive capacities, increased reaction time, and decreased spinal-stretch reflex
11 system function [1-3]. These deteriorations could possibly put elderly individuals at greater
12 risk of falls [2]. To address the issue of decreased functionality of postural regulation, lower-
13 limb stimulation strategies (LLS) such as wearable garments (braces & socks) [5,6], textured
14 insoles [6,7] and application of Stochastic Resonance (SR) [6] have demonstrated some
15 positive effects on postural regulation during balancing tasks in middle-aged and older adults
16 (65 years and above). On the other hand, postural regulation and stability are affected by the
17 types of standing surfaces and the visual conditions available to a person (Patel et al., 2008).
18 Specifically, foam surfaces are commonly used to disrupt somatosensory information (Patel
19 et al. 2008; Qiu et al., 2012). With the absence of vision, studies have suggested that postural
20 sway increases, especially when individuals are standing on a foam surface (Patel et al.,
21 2008; Vuillerman & Pinsault, 2007). However, further investigation of elderly samples are
22 needed to ascertain whether postural regulation can be enhanced during static balance, when
23 standing on different surfaces and under varied visual conditions (e.g., with and without),
24 when wearing compression socks. Therefore, this study aimed to investigate the effects of

1 compression wearable garments on somatosensory feedback in static balance task, under
2 different standing surfaces and vision conditions (e.g., with and without), in elderly people.

3 An ecological dynamics framework has been proposed to account for how
4 compression and textured materials can support the exploitation of sensorimotor system noise
5 to enhance functional performance. Davids et al. (2003) [9] argued that the functional role of
6 variability induced in the sensorimotor system by textured insoles, acts as a form of “essential
7 noise” which helps individuals regulate actions. They suggested that the addition of
8 intermittent, intermediate levels of noise, via textured insoles, may help performers to pick up
9 information from the background signals to enhance perception of somatosensory feedback
10 [9]. Effects of wearable garments could be related to neuromotor function, specifically
11 invoking the Hoffmann Reflex (H-reflex), an indirect measure of motorneuron excitability
12 [14]. It has been reported that wearing an ankle brace increases motorneuron excitation in the
13 afferent system at the Peroneus Longus muscle [14], providing additional active impact for
14 proprioceptive control of movement in the ankle dorsiflexor muscles [15]. Evidence from
15 research on performance of a younger, athletic population performing a sport action implies
16 that stimulation of the sensory system in the lower limbs by wearable garments (e.g.,
17 compression socks and textured insoles) could potentially increase the efficiency of
18 somatosensory system function and aid postural regulation of elderly individuals [17].

19 It has also been suggested that application of stimulation, provided by adding
20 pressure, texture nodules, and velcro strapping on the cutaneous, joint and muscle receptors
21 of the lower limbs could enhance the level of sensorimotor system noise to improve
22 perceptual-motor system functionality [6,7,9-11]. A postulation is that stimulation of the
23 muscle spindles and mechanoreceptors along the shank, when wearing compression socks,
24 enhances postural regulation by contortion and disturbances of haptic system receptors in the
25 skin and soft tissue of the lower limbs [6]. Recent investigations have suggested some

1 beneficial effects of wearing a knee compressive sleeve in reducing postural sway in the
2 anteroposterior (AP) direction [22], and donning a compression stocking reduced the CoP
3 trajectory amplitude [21]. In an elderly sample, Losa Iglesia (2012) [25] reported that
4 wearing socks reduced sway areas compared to when the same participants regulated posture
5 in a barefoot condition. These initial findings suggest that more research is needed to address
6 the role of wearing compression socks in stimulating somatosensory system feedback that
7 emerges from pressure on cutaneous and joint receptors in the lower legs in the elderly
8 population.

9 Furthermore, no studies have addressed the question of effects of LLS related to
10 gender differences associated with age-related degeneration of the perceptual-motor system.
11 It is possible that elderly men and women respond differently, based on fundamental
12 differences in morphology, exemplified by variations in brain structure and function,
13 musculature and the sensory systems [26]. For example, some studies have identified a
14 possible gender effect with elderly women displaying greater CoP sway values [27], lower
15 balance scores [28], and shorter nerve conduction pathways [26], than elderly men. Wearing
16 compression garments could potentially enhance the sensitivity of the cutaneous and
17 mechanoreceptors in elderly females, reducing their falls risk, by indirectly enhancing their
18 postural regulation capacity. on.

19 Therefore, the current study sought to understand whether wearing compressive knee
20 length socks (KLS) would enhance the stimulation of mechanoreceptors in the lower limbs of
21 elderly men and women, helping these community-dwelling individuals to achieve better
22 postural regulation, and potentially forming a strategy to reduce risk of falling.

23 .

24 We sought to add to the literature by discerning the impact of low cost, easily
25 implemented compression materials, on somatosensory function and postural regulation in

1 elderly males and females. The specific aim of this study was to examine immediate effects
2 of wearing KLS of various compression levels on postural regulation under four levels of
3 performance difficulty, in community-dwelling healthy elderly men and women, during
4 double-limb standing, balancing task. It was hypothesized that wearing compression KLS
5 would reduce postural sway, with gender-based differences being observed in these
6 community-dwelling elderly men and women.

7 **2.0 Methods**

8 *2.1 Participants*

9 A total of 46 (Male = 23) community-dwelling elderly individuals (Table 1), were
10 randomly selected based on specific inclusion criteria, from the profiling of Singapore
11 community-dwelling elderly people project [28]. Specific inclusion criteria were ability to
12 walk independently without using any assistive devices (e.g., walking stick; umbrella), no
13 history of falling in the past 12 months, Berg Balance task Score > 40 (normal), and Mini-
14 Mental State Examination (MMSE) score > 24 (normal). Exclusion criteria were: evidence of
15 muscular and neurological diseases, recent stroke events (< 18 months), and brain injuries.
16 Voluntary and informed consent was obtained from all 46 participants, and the procedures
17 used in the study were approved and in accordance with the ethical guidelines of the research
18 ethics committee of Nanyang Technological University, Singapore.

19
20 ***Insert Table 1 about here***
21

22 *2.2 Apparatus and Tasks*

23 Three treatment interventions (wearing clinical compression KLS; wearing non-
24 clinical compression KLS; wearing commercial KLS) and one control condition (barefoot), in
25 a counterbalanced order, were administered to participants while they performed a double-
26 limb standing balance task. In testing we used KLS with clinical level compression KLS (CC)

1 of 20-30 mmHg pressure (Zeropoint, Finland), KLS with non-clinical level compression
2 (NCC) of 8-15mmHg (X-bionic, Switzerland), and non-compression (NC) models
3 commercial KLS (Mizuno, Japan) of similar thickness The purpose of including different
4 types of KLS was to gain insights into effects of wearing garments of varying compression
5 levels. We sought to discern whether the degree of contortion of lower limb tissue, by
6 different compression properties, might influence postural regulation function in elderly
7 males and females. The tasks required participants to perform a 30-s Romberg test on a
8 balance platform (Hur, Finland) under two vision conditions (eyes open and closed) and on
9 two standing surfaces (stable and foam) inside a laboratory. The dimension of the foam was
10 50 x 50 x 10 cm and the density was at 30 kg/m³.

11 The four levels of performance difficulty task conditions were standing on: (1) a
12 stable surface with eyes open (SO); (2) a stable surface with eyes closed (SC); (3) a foam
13 surface with eyes open (FO); and (4), a foam surface with eyes closed (FC). All treatment
14 interventions and task conditions were presented in a random order for each participant.

15

16 *2.3 Procedure*

17 A repeated-measures design was used to determine effects on balance and postural
18 control of four different treatment conditions – wearing CC KLS; wearing NCC KLS;
19 wearing NC KLS; barefoot. The sequences of the testing interventions and the task conditions
20 were randomised by using Microsoft Excel to prevent carryover/order effects.

21 For the 30-s Romberg test, participants were instructed to stand upright and as still as
22 possible with feet together and the arms by the side. For the eyes open condition, participants
23 were asked to look straight ahead to a reference point on a blank wall, marked at eye level,
24 and it was about 1.5 m away from the balance platform. For the unstable surface, a 10-cm

1 thick foam pad was placed on top of the balance platform to create a more challenging
2 surface for the participants.

3 Before data collection, participants undertook two trials of the static balance task to
4 familiarize themselves with each of the four task conditions– SO, SC FO, FC. For every
5 treatment intervention, participants were required to perform 2 trials for each of the task
6 conditions. Participants were given a sufficient rest period (~ 2 minutes) between each
7 treatment intervention. The tests were repeated if participants lost balance on the platform.

8

9 *2.4 Data processing and Statistical analysis*

10 Centre of pressure data were collected at a sampling frequency of 100Hz,
11 accumulating to 3000 data points for each condition. The parameters were the 90%
12 confidence elliptical area (C90 sway area), trace length (TL, the total length of the CoP path),
13 sway velocity, range of anterior–posterior (AP) and medial–lateral (ML) CoP displacement,
14 AP and ML standard deviation (SD). Observed increases in value of these parameters were
15 associated with a greater risk of falling [29]. It has been reported that the sway area, trace
16 length, and sway velocity are the most reliable CoP stabilometric parameters in measuring
17 postural stability [3]. All data were analyzed by using nonparametric statistical tests due to
18 abnormal data distributions. SPSS software (version 24.0) was used for statistical analysis.
19 All measurements across the treatment interventions were compared using a Friedman test –
20 K related samples. If statistically significant results were found during the Friedman test,
21 Wilcoxon sign test was conducted to further identify which treatment intervention resulted in
22 a significant effect. Results were reported as means and standard deviation (SD). Alpha level
23 was set at <0.05 for all statistical analyses.

24

25

3.0 Results

1 *3.1 Postural sway (C90) area*

2 For the female group, the Friedman test revealed significant differences across the treatment
3 interventions on the foam surface with eyes open ($p = 0.007$) (Figure 1). Post hoc analysis
4 showed that the sway area in that group was significantly lower while wearing the NCC ($p =$
5 0.013) and NC ($p = 0.016$) KLS compared to the barefoot condition. No statistically significant
6 effects were found across the treatment interventions in men.

7

8 ***Insert Figure 1 about here***

9

10

11 *3.2 Trace length*

12 For the female group, the Friedman test revealed significant differences across the treatment
13 interventions on the foam surface with eyes open ($p = 0.007$), but not in the other three task
14 conditions – SO, SC and FC (Figure 2). Post hoc analysis showed that trace length was
15 significantly shorter while participants wore the NCC KLS ($p = 0.013$), compared to the
16 barefoot condition for the FO task condition. No statistically significant effects were found
17 across the treatment interventions in men.

18

19 ***Insert Figure 2 about here***

20

21

22 *3.3 Sway velocity*

23 The Friedman test revealed significant differences across the treatment interventions ($p =$
24 0.027) in the female group in the FO task condition (Figure 3). Post hoc analysis showed that
25 sway velocity was significantly lower while wearing the CC and NCC KLS ($p = 0.013$)
26 compared to the barefoot condition. No statistically significant effects were found across the
27 treatment interventions in men.

28

1 ***Insert Figure 3 about here***
2
3

4 *3.4 Anterior–posterior (AP) postural sway and AP SD*

5 There were significant differences across the treatment interventions in AP sway on both stable
6 ($p = 0.043$) and foam ($p = 0.027$) surfaces, with eyes open (Table 2) in the elderly males. In the
7 SO task condition, post hoc analysis revealed that CC KLS significantly decreased AP sway
8 compared to when wearing NCC KLS ($p = 0.013$) and when standing barefoot ($p = 0.039$) in
9 the elderly men. The same beneficial effect of wearing CC KLS was observed in the FO
10 condition. A significant difference across treatment interventions was observed on APSD ($p =$
11 0.012) in the SC condition. However, no significant differences were found in all treatment
12 interventions and all task conditions on AP sway and AP SD values in the women.

14 *3.5 Medial–lateral (ML) postural sway and ML SD*

15 There were no differences across the treatment interventions on ML sway and ML SD in the
16 elderly men (Table 2). A significant difference across treatment conditions was observed in
17 MLSD ($p = 0.012$) in SC task in the women.

18
19 ***Insert Table 2 about here***
20
21

22 **4.0 Discussion**

24 The aim of this study was to examine immediate effects of wearing KLS of various
25 compression levels on somatosensory function, during a double-limb standing balancing task.
26 The results of this study support our hypothesis on the beneficial effects of wearing
27 compression KLS on postural regulation in community-dwelling elderly men and women. In
28 elderly men, wearing CC and NCC KLS decreased postural sway, mainly in the AP direction

1 in both SO and FO task conditions. Similarly, wearing KLS, particularly non-clinical
2 compression, reduced sway area, trace length and sway velocity while standing on the foam
3 surface with eyes open (FO) in the elderly women. There were no significant beneficial
4 effects of all levels of KLS observed in the FC condition in both elderly men and women.

5 Consistent with findings of previous studies, use of lower-limb stimulation strategies
6 decreased postural sway for elderly participants wearing textured insoles (see Qiu et al.,
7 2012) and hard insoles (Losa Iglesia et al., 2012). Our results support the idea that
8 compression wearable garments can enhance the functioning of the postural regulation
9 system by reducing sway [6,11,21,23]. Wearing CC and NCC KLS are deemed to be
10 beneficial perhaps due to their capacity to support exploitation of the available “sensorimotor
11 system noise” to enhance perception of proprioceptive and haptic information during
12 performance of complex tasks (for example, maintaining upright stance while standing on an
13 unstable surface). Furthermore, wearing compression KLS yielded similar effects as balance
14 training interventions (electrical stimulation) in improving postural stability in elderly people
15 [16,30]. Perhaps wearing compression KLS may increased d motorneuron excitability of H-
16 reflex, as suggested by Nishikawa and Grabiner (1999) and down-modulated the Hoffmann
17 Reflex (H-reflex). Therefore, wearing compression KLS, which covered most of the lower
18 legs, seemed to stimulate the various cutaneous mechanoreceptors, motor neuron and muscle
19 proprioceptors along the shanks, and could potentially form a strategy to ameliorate negative
20 effects of ageing on the postural control system and reduce risk of falling

21 The amplitude and conduction velocity of motor and sensory nerves have been found
22 to significantly differ with gender (Jha, 2018; Pelliccioni et al., 2014). This effect could be
23 potentially attributed to the gender-based differences observed from wearing the compression
24 KLS in our study. In agreement with our findings, Olchowik et al. (2015) found that men
25 displayed less postural sway than women in the AP direction. Our findings provided new

1 insights, indicating that wearing compression KLS, is beneficial to men, as supported by the
2 decrease in the sway distance in the AP direction. Furthermore, we found that women
3 displayed positive performance outcome in many COP variables such as sway area, trace
4 length and sway velocity. This observation could be due to the possibility that women use the
5 ankle strategy (to regulate balance) more effectively than men (Olchowik et al., 2015;
6 Pelliccioni et al., 2014). Wearing compression KLS seems to aid the ankle control strategy by
7 stimulating the cutaneous and mechanoreceptors around the ankle joint. An issue requiring
8 further research concerns the suggestion that compression garment manufacturers may
9 improve sock design, by concentrating the stimulating material (by increasing textured
10 undulations) surrounding the ankle and at the anterior-posterior aspects of the compression
11 socks.

12 In this study, KLS enhanced postural regulation performance in a challenging
13 condition – during upright balance on a foam (unstable) surface with eyes open (i.e.,
14 availability of vision), supporting findings with textured insoles reported by Qiu et al. (2012).
15 The role of somatosensory feedback is assumed to be more important when standing on an
16 unstable surface (Patel et al., 2008 [24]. In the current study, wearing compression KLS
17 seemed to provide necessary sensory information to the Central Nervous System (CNS) and
18 facilitated the perceptual regulation of stance [24] when the somatosensory system is
19 compromised. In contrast to data of Qiu et al. (2017), our study showed no immediate
20 beneficial effects of wearing compression KLS when both vision and somatosensory are
21 compromised [i.e., standing on a foam surface with eyes closed (FC)]. Effects of these
22 sensory perturbations seemed to be too severe for mediation by wearing compression
23 garments, although potential long term effects may need to be assessed. This finding could
24 imply that the somatosensory system stimulation provided by wearing compression KLS is
25 not sufficient to yield beneficial effects when both vision and somatosensory systems are

1 compromised. However, more studies are needed to confirm the beneficial effects of wearing
2 compression KLS on postural regulation in the FC condition.

3 To summarise, our study showed that wearing compression KLS significantly
4 improved the balance performance in FO task condition. It was observed that men and
5 women responded differently to the effects of wearing compression KLS on postural
6 regulation. Wearing compression KLS could be used as a medium to reduce risk of falling
7 and enhance postural control and function of the perceptual-motor systems. A limitation of
8 this study includes the absence of an assessment of the muscle strength capacity of our
9 participants and it is unknown whether individual variations in lower limb muscle strength
10 affected performance outcomes, if at all. Future studies could include some form of
11 measurement of muscle strength to determine the effect of muscle strength coupled with the
12 use of KLS on the balance tasks. In addition, there could also be an emphasis on examining
13 the long-term effects of wearing compression KLS on postural regulation and dynamic tasks
14 (e.g., walking, sliding), and the immediate effects of wearing compression KLS in specific
15 groups of elderly individuals with debilitating conditions, such as diabetes, Parkinson Disease
16 and peripheral neuropathy.

17

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