

# Immediate effects of wearing knee length socks differing in compression level on postural regulation in communitydwelling, healthy, elderly men and women

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| 1  | Immediate effects of wearing knee length socks differing in compression level on              |
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| 2  | postural regulation in community-dwelling, healthy, elderly men and women                     |
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1 Postural regulation and stability of balance are affected by types of standing surfaces 2 and somatosensory system function of an individual (Patel et al., 2008). Standing on unstable 3 surfaces, like foam surfaces, have revealed the important role of somatosensory information 4 in postural regulation and balance (Patel et al. 2008; Qiu et al., 2012). Studies have suggested 5 that postural sway increases for balance regulation, especially when individuals are standing 6 on a foam surface (Patel et al., 2008; Vuillerman & Pinsault, 2007). Somatosensory function 7 is important to study since neurodegeneration can result in age-related declines in postural 8 regulation due to reduction in cognitive and sensory system capacities (Rose, 2012). For 9 example, ageing can result in decreased sensitivity to sensory information and motor output, 10 slowing of cognitive capacities, increased reaction time, and decreased spinal-stretch reflex 11 system function [1-3]. These deteriorations could possibly put elderly individuals at greater 12 risk of falls [2]. To address the issue of decreased functionality of postural regulation, lower-13 limb stimulation strategies (LLS) such as wearable garments (braces & socks) [5,6], textured 14 insoles [6,7] and application of Stochastic Resonance (SR) [6] have demonstrated some 15 positive effects on postural regulation during balancing tasks in middle-aged and older adults 16 (65 years and above). On the other hand, postural regulation and stability are affected by the 17 types of standing surfaces and the visual conditions available to a person (Patel et al., 2008). 18 Specifically, foam surfaces are commonly used to disrupt somatosensory information (Patel 19 et al. 2008; Qiu et al., 2012). With the absence of vision, studies have suggested that postural 20 sway increases, especially when individuals are standing on a foam surface (Patel et al., 21 2008; Vuillerman & Pinsault, 2007). However, further investigation of elderly samples are 22 needed to ascertain whether postural regulation can be enhanced during static balance, when 23 standing on different surfaces and under varied visual conditions (e.g., with and without), 24 when wearing compression socks. Therefore, this study aimed to investigate the effects of

1 compression wearable garments on somatosensory feedback in static balance task, under 2 different standing surfaces and vision conditions (e.g., with and without), in elderly people. 3 An ecological dynamics framework has been proposed to account for how 4 compression and textured materials can support the exploitation of sensorimotor system noise 5 to enhance functional performance. Davids et al. (2003) [9] argued that the functional role of 6 variability induced in the sensorimotor system by textured insoles, acts as a form of "essential 7 noise" which helps individuals regulate actions. They suggested that the addition of 8 intermittent, intermediate levels of noise, via textured insoles, may help performers to pick up 9 information from the background signals to enhance perception of somatosensory feedback 10 [9]. Effects of wearable garments could be related to neuromotor function, specifically 11 invoking the Hoffmann Reflex (H-reflex), an indirect measure of motorneuron excitability 12 [14]. It has been reported that wearing an ankle brace increases motorneuron excitation in the 13 afferent system at the Peroneus Longus muscle [14], providing additional active impact for 14 proprioceptive control of movement in the ankle dorsiflexor muscles [15]. Evidence from 15 research on performance of a younger, athletic population performing a sport action implies 16 that stimulation of the sensory system in the lower limbs by wearable garments (e.g., 17 compression socks and textured insoles) could potentially increase the efficiency of 18 somatosensory system function and aid postural regulation of elderly individuals [17]. 19 It has also been suggested that application of stimulation, provided by adding 20 pressure, texture nodules, and velcro strapping on the cutaneous, joint and muscle receptors 21 of the lower limbs could enhance the level of sensorimotor system noise to improve 22 perceptual-motor system functionality [6,7,9-11]. A postulation is that stimulation of the 23 muscle spindles and mechanoreceptors along the shank, when wearing compression socks, 24 enhances postural regulation by contortion and disturbances of haptic system receptors in the 25 skin and soft tissue of the lower limbs [6]. Recent investigations have suggested some

1 beneficial effects of wearing a knee compressive sleeve in reducing postural sway in the 2 anteroposterior (AP) direction [22], and donning a compression stocking reduced the CoP 3 trajectory amplitude [21]. In an elderly sample, Losa Iglesia (2012) [25] reported that 4 wearing socks reduced sway areas compared to when the same participants regulated posture 5 in a barefoot condition. These initial findings suggest that more research is needed to address 6 the role of wearing compression socks in stimulating somatosensory system feedback that 7 emerges from pressure on cutaneous and joint receptors in the lower legs in the elderly 8 population.

9 Furthermore, no studies have addressed the question of effects of LLS related to 10 gender differences associated with age-related degeneration of the perceptual-motor system. 11 It is possible that elderly men and women respond differently, based on fundamental 12 differences in morphology, exemplified by variations in brain structure and function, 13 musculature and the sensory systems [26]. For example, some studies have identified a 14 possible gender effect with elderly women displaying greater CoP sway values [27], lower 15 balance scores [28], and shorter nerve conduction pathways [26], than elderly men. Wearing 16 compression garments could potentially enhance the sensitivity of the cutaneous and 17 mechanoreceptors in elderly females, reducing their falls risk, by indirectly enhancing their 18 postural regulation capacity. on.

19 Therefore, the current study sought to understand whether wearing compressive knee 20 length socks (KLS) would enhance the stimulation of mechanoreceptors in the lower limbs of 21 elderly men and women, helping these community-dwelling individuals to achieve better 22 postural regulation, and potentially forming a strategy to reduce risk of falling.

23

We sought to add to the literature by discerning the impact of low cost, easily
implemented compression materials, on somatosensory function and postural regulation in

elderly males and females. The specific aim of this study was to examine immediate effects
of wearing KLS of various compression levels on postural regulation under four levels of
performance difficulty, in community-dwelling healthy elderly men and women, during
double-limb standing, balancing task. It was hypothesized that wearing compression KLS
would reduce postural sway, with gender-based differences being observed in these
community-dwelling elderly men and women.

7

### 2.0 Methods

8 2.1 Participants

9 A total of 46 (Male = 23) community-dwelling elderly individuals (Table 1), were 10 randomly selected based on specific inclusion criteria, from the profiling of Singapore 11 community-dwelling elderly people project [28]. Specific inclusion criteria were ability to 12 walk independently without using any assistive devices (e.g., walking stick; umbrella), no 13 history of falling in the past 12 months, Berg Balance task Score > 40 (normal), and Mini-14 Mental State Examination (MMSE) score > 24 (normal). Exclusion criteria were: evidence of 15 muscular and neurological diseases, recent stroke events (< 18 months), and brain injuries. 16 Voluntary and informed consent was obtained from all 46 participants, and the procedures 17 used in the study were approved and in accordance with the ethical guidelines of the research 18 ethics committee of Nanyang Technological University, Singapore.

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#### \*\*\*Insert Table 1 about here\*\*\*

22 2.2 Apparatus and Tasks

Three treatment interventions (wearing clinical compression KLS; wearing nonclinical compression KLS; wearing commercial KLS) and one control condition (barefoot), in a counterbalanced order, were administered to participants while they performed a doublelimb standing balance task. In testing we used KLS with clinical level compression KLS (CC)

1 of 20-30 mmHg pressure (Zeropoint, Finland), KLS with non-clinical level compression 2 (NCC) of 8-15mmHg (X-bionic, Switzerland), and non-compression (NC) models 3 commercial KLS (Mizuno, Japan) of similar thickness The purpose of including different 4 types of KLS was to gain insights into effects of wearing garments of varying compression 5 levels. We sought to discern whether the degree of contortion of lower limb tissue, by different compression properties, might influence postural regulation function in elderly 6 7 males and females. The tasks required participants to perform a 30-s Romberg test on a 8 balance platform (Hur, Finland) under two vision conditions (eyes open and closed) and on 9 two standing surfaces (stable and foam) inside a laboratory. The dimension of the foam was 10  $50 \times 50 \times 10$  cm and the density was at  $30 \text{ kg/m}^3$ . 11 The four levels of performance difficulty task conditions were standing on: (1) a 12 stable surface with eyes open (SO); (2) a stable surface with eyes closed (SC); (3) a foam 13 surface with eyes open (FO); and (4), a foam surface with eyes closed (FC). All treatment 14 interventions and task conditions were presented in a random order for each participant. 15 16 2.3 Procedure 17 A repeated-measures design was used to determine effects on balance and postural 18 control of four different treatment conditions - wearing CC KLS; wearing NCC KLS; 19 wearing NC KLS; barefoot. The sequences of the testing interventions and the task conditions 20 were randomised by using Microsoft Excel to prevent carryover/order effects. 21 For the 30-s Romberg test, participants were instructed to stand upright and as still as 22 possible with feet together and the arms by the side. For the eyes open condition, participants 23 were asked to look straight ahead to a reference point on a blank wall, marked at eye level, 24 and it was about 1.5 m away from the balance platform. For the unstable surface, a 10-cm

1 thick foam pad was placed on top of the balance platform to create a more challenging 2 surface for the participants.

3 Before data collection, participants undertook two trials of the static balance task to 4 familiarize themselves with each of the four task conditions- SO, SC FO, FC. For every 5 treatment intervention, participants were required to perform 2 trials for each of the task 6 conditions. Participants were given a sufficient rest period (~ 2 minutes) between each 7 treatment intervention. The tests were repeated if participants lost balance on the platform. 8

#### 9 2.4 Data processing and Statistical analysis

10 Centre of pressure data were collected at a sampling frequency of 100Hz, 11 accumulating to 3000 data points for each condition. The parameters were the 90% 12 confidence elliptical area (C90 sway area), trace length (TL, the total length of the CoP path), 13 sway velocity, range of anterior-posterior (AP) and medial-lateral (ML) CoP displacement, 14 AP and ML standard deviation (SD). Observed increases in value of these parameters were 15 associated with a greater risk of falling [29]. It has been reported that the sway area, trace 16 length, and sway velocity are the most reliable CoP stabilometric parameters in measuring 17 postural stability [3]. All data were analyzed by using nonparametric statistical tests due to 18 abnormal data distributions. SPSS software (version 24.0) was used for statistical analysis. 19 All measurements across the treatment interventions were compared using a Friedman test – 20 K related samples. If statistically significant results were found during the Friedman test, 21 Wilcoxon sign test was conducted to further identify which treatment intervention resulted in 22 a significant effect. Results were reported as means and standard deviation (SD). Alpha level 23 was set at <0.05 for all statistical analyses.

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### 3.0 Results

## 1 3.1 Postural sway (C90) area

| 2                    | For the female group, the Friedman test revealed significant differences across the treatment      |
|----------------------|--|
| 3                    | interventions on the foam surface with eyes open ( $p = 0.007$ ) (Figure 1). Post hoc analysis     |
| 4                    | showed that the sway area in that group was significantly lower while wearing the NCC ( $p =$      |
| 5                    | 0.013) and NC ( $p = 0.016$ ) KLS compared to the barefoot condition. No statistically significant |
| 6                    | effects were found across the treatment interventions in men.                                      |
| 7                    |  |
| 8<br>9<br>10         | ***Insert Figure 1 about here***   |
| 11                   | 3.2 Trace length   |
| 12                   | For the female group, the Friedman test revealed significant differences across the treatment      |
| 13                   | interventions on the foam surface with eyes open ( $p = 0.007$ ), but not in the other three task  |
| 14                   | conditions – SO, SC and FC (Figure 2). Post hoc analysis showed that trace length was              |
| 15                   | significantly shorter while participants wore the NCC KLS ( $p = 0.013$ ), compared to the         |
| 16                   | barefoot condition for the FO task condition. No statistically significant effects were found      |
| 17                   | across the treatment interventions in men.   |
| 18                   |  |
| 19<br>20<br>21<br>22 | ***Insert Figure 2 about here*** 3.3 Sway velocity   |
| 23                   | The Friedman test revealed significant differences across the treatment interventions (p =         |
| 24                   | 0.027) in the female group in the FO task condition (Figure 3). Post hoc analysis showed that      |
| 25                   | sway velocity was significantly lower while wearing the CC and NCC KLS ( $p = 0.013$ )             |
| 26                   | compared to the barefoot condition. No statistically significant effects were found across the     |
| 27                   | treatment interventions in men.  |
| 28                   |  |

\*\*\*Insert Figure 3 about here\*\*\* 1 2 3 4 3.4 Anterior-posterior (AP) postural sway and AP SD 5 There were significant differences across the treatment interventions in AP sway on both stable 6 (p = 0.043) and foam (p = 0.027) surfaces, with eyes open (Table 2) in the elderly males. In the 7 SO task condition, post hoc analysis revealed that CC KLS significantly decreased AP sway 8 compared to when wearing NCC KLS (p = 0.013) and when standing barefoot (p = 0.039) in 9 the elderly men. The same beneficial effect of wearing CC KLS was observed in the FO 10 condition. A significant difference across treatment interventions was observed on APSD (p = 11 0.012) in the SC condition. However, no significant differences were found in all treatment 12 interventions and all task conditions on AP sway and AP SD values in the women. 13 14 3.5 Medial-lateral (ML) postural sway and ML SD 15 There were no differences across the treatment interventions on ML sway and ML SD in the 16 elderly men (Table 2). A significant difference across treatment conditions was observed in 17 MLSD (p = 0.012) in SC task in the women. 18 19 \*\*\*Insert Table 2 about here\*\*\* 20 21 22 23 4.0 Discussion 24 The aim of this study was to examine immediate effects of wearing KLS of various 25 compression levels on somatosensory function, during a double-limb standing balancing task. 26 The results of this study support our hypothesis on the beneficial effects of wearing 27 compression KLS on postural regulation in community-dwelling elderly men and women. In 28 elderly men, wearing CC and NCC KLS decreased postural sway, mainly in the AP direction

1 in both SO and FO task conditions. Similarly, wearing KLS, particularly non-clinical 2 compression, reduced sway area, trace length and sway velocity while standing on the foam 3 surface with eyes open (FO) in the elderly women. There were no significant beneficial 4 effects of all levels of KLS observed in the FC condition in both elderly men and women. 5 Consistent with findings of previous studies, use of lower-limb stimulation strategies 6 decreased postural sway for elderly participants wearing textured insoles (see Qiu et al., 7 2012) and hard insoles (Losa Iglesia et al., 2012). Our results support the idea that 8 compression wearable garments can enhance the functioning of the postural regulation 9 system by reducing sway [6,11,21,23]. Wearing CC and NCC KLS are deemed to be 10 beneficial perhaps due to their capacity to support exploitation of the available "sensorimotor 11 system noise" to enhance perception of proprioceptive and haptic information during 12 performance of complex tasks (for example, maintaining upright stance while standing on an 13 unstable surface). Furthermore, wearing compression KLS yielded similar effects as balance 14 training interventions (electrical stimulation) in improving postural stability in elderly people 15 [16,30]. Perhaps wearing compression KLS may increased d motorneuron excitability of H-16 reflex, as suggested by Nishikawa and Grabiner (1999) and down-modulated the Hoffmann 17 Reflex (H-reflex). Therefore, wearing compression KLS, which covered most of the lower 18 legs, seemed to stimulate the various cutaneous mechanoreceptors, motor neuron and muscle 19 proprioceptors along the shanks, and could potentially form a strategy to ameliorate negative 20 effects of ageing on the postural control system and reduce risk of falling 21 The amplitude and conduction velocity of motor and sensory nerves have been found 22 to significantly differ with gender (Jha, 2018; Pelliccioni et al., 2014). This effect could be 23 potentially attributed to the gender-based differences observed from wearing the compression 24 KLS in our study. In agreement with our findings, Olchowik et al. (2015) found that men

25 displayed less postural sway than women in the AP direction. Our findings provided new

1 insights, indicating that wearing compression KLS, is beneficial to men, as supported by the 2 decrease in the sway distance in the AP direction. Furthermore, we found that women 3 displayed positive performance outcome in many COP variables such as sway area, trace 4 length and sway velocity. This observation could be due to the possibility that women use the 5 ankle strategy (to regulate balance) more effectively than men (Olchowik et al., 2015; 6 Pelliccioni et al., 2014). Wearing compression KLS seems to aid the ankle control strategy by 7 stimulating the cutaneous and mechanoreceptors around the ankle joint. An issue requiring 8 further research concerns the suggestion that compression garment manufacturers may 9 improve sock design, by concentrating the stimulating material (by increasing textured 10 undulations) surrounding the ankle and at the anterior-posterior aspects of the compression 11 socks.

12 In this study, KLS enhanced postural regulation performance in a challenging 13 condition - during upright balance on a foam (unstable) surface with eyes open (i.e., 14 availability of vision), supporting findings with textured insoles reported by Qiu et al. (2012). 15 The role of somatosensory feedback is assumed to be more important when standing on an 16 unstable surface (Patel et al., 2008 [24]. In the current study, wearing compression KLS 17 seemed to provide necessary sensory information to the Central Nervous System (CNS) and 18 facilitated the perceptual regulation of stance [24] when the somatosensory system is 19 compromised. In contrast to data of Qiu et al. (2017), our study showed no immediate 20 beneficial effects of wearing compression KLS when both vision and somatosensory are 21 compromised [i.e., standing on a foam surface with eyes closed (FC)]. Effects of these 22 sensory perturbations seemed to be too severe for mediation by wearing compression 23 garments, although potential long term effects may need to be assessed. This finding could 24 imply that the somatosensory system stimulation provided by wearing compression KLS is 25 not sufficient to yield beneficial effects when both vision and somatosensory systems are

compromised. However, more studies are needed to confirm the beneficial effects of wearing
 compression KLS on postural regulation in the FC condition.

- 3 To summarise, our study showed that wearing compression KLS significantly improved the balance performance in FO task condition. It was observed that men and 4 5 women responded differently to the effects of wearing compression KLS on postural 6 regulation. Wearing compression KLS could be used as a medium to reduce risk of falling 7 and enhance postural control and function of the perceptual-motor systems. A limitation of 8 this study includes the absence of an assessment of the muscle strength capacity of our 9 participants and it is unknown whether individual variations in lower limb muscle strength 10 affected performance outcomes, if at all. Future studies could include some form of 11 measurement of muscle strength to determine the effect of muscle strength coupled with the 12 use of KLS on the balance tasks. In addition, there could also be an emphasis on examining 13 the long-term effects of wearing compression KLS on postural regulation and dynamic tasks 14 (e.g., walking, sliding), and the immediate effects of wearing compression KLS in specific 15 groups of elderly individuals with debilitating conditions, such as diabetes, Parkinson Disease 16 and peripheral neuropathy. 17
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